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(54) **X-RAY DIAGNOSIS APPARATUS AND X-RAY
DIAGNOSIS ASSISTING METHOD**

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filed on Apr. 25, 2013.

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A61B 6/12 (2006.01)
(Continued)

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CPC ... **A61B 6/10** (2013.01); **A61B 6/06** (2013.01);
A61B 6/12 (2013.01); **A61B 6/487** (2013.01);
A61B 6/542 (2013.01)

(58) **Field of Classification Search**

CPC A61B 6/487; A61B 6/12; A61B 6/504;
A61B 6/542

USPC 378/42, 147-153
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

7,539,284 B2 * 5/2009 Besson 378/62
2011/0013742 A1 * 1/2011 Zaiki et al. 378/15
2012/0189093 A1 7/2012 Zaiki et al.

FOREIGN PATENT DOCUMENTS

CN 101953691 A 1/2011
JP 63-286170 11/1988

(Continued)

OTHER PUBLICATIONS

International Search Report issued on Jun. 18, 2013 for PCT/JP2013/
002814 filed on Apr. 25, 2013 with English Translation of Categories.

(Continued)

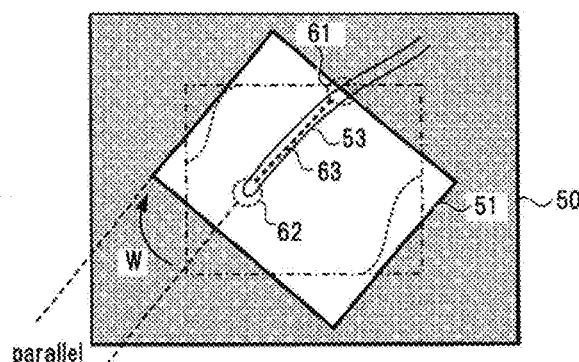
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(57) **ABSTRACT**

An X-ray diagnosis apparatus of an embodiment includes: an imaging unit that includes an X-ray tube which emits an X-ray to a subject, and an X-ray detector which detects an X-ray passing through the subject; an X-ray beam limiting unit that is disposed between the X-ray tube and the X-ray detector, has a plurality of collimator blades, and can be rotated; an image processing unit that generates a fluoroscopic image of a region of interest set by the X-ray beam limiting unit; and a control unit that individually controls the plurality of collimator blades in such a way that a long side of an opening formed by the plurality of collimator blades goes in a longitudinal direction of a target within the fluoroscopic image.

10 Claims, 15 Drawing Sheets



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(56) **References Cited**

FOREIGN PATENT DOCUMENTS

JP 2011-19633 2/2011
JP 2012-75782 4/2012

OTHER PUBLICATIONS

International Written Opinion issued on Jun. 18, 2013 for PCT/
JP2013/002814 filed on Apr. 25, 2013.
Office Action issued Feb. 16, 2015 in Chinese Patent Application No.
201380000559.8 (with partial English translation).
Search Report issued Feb. 5, 2015 in Chinese Patent Application No.
201380000559.8 (with partial English translation).

* cited by examiner

FIG. 1

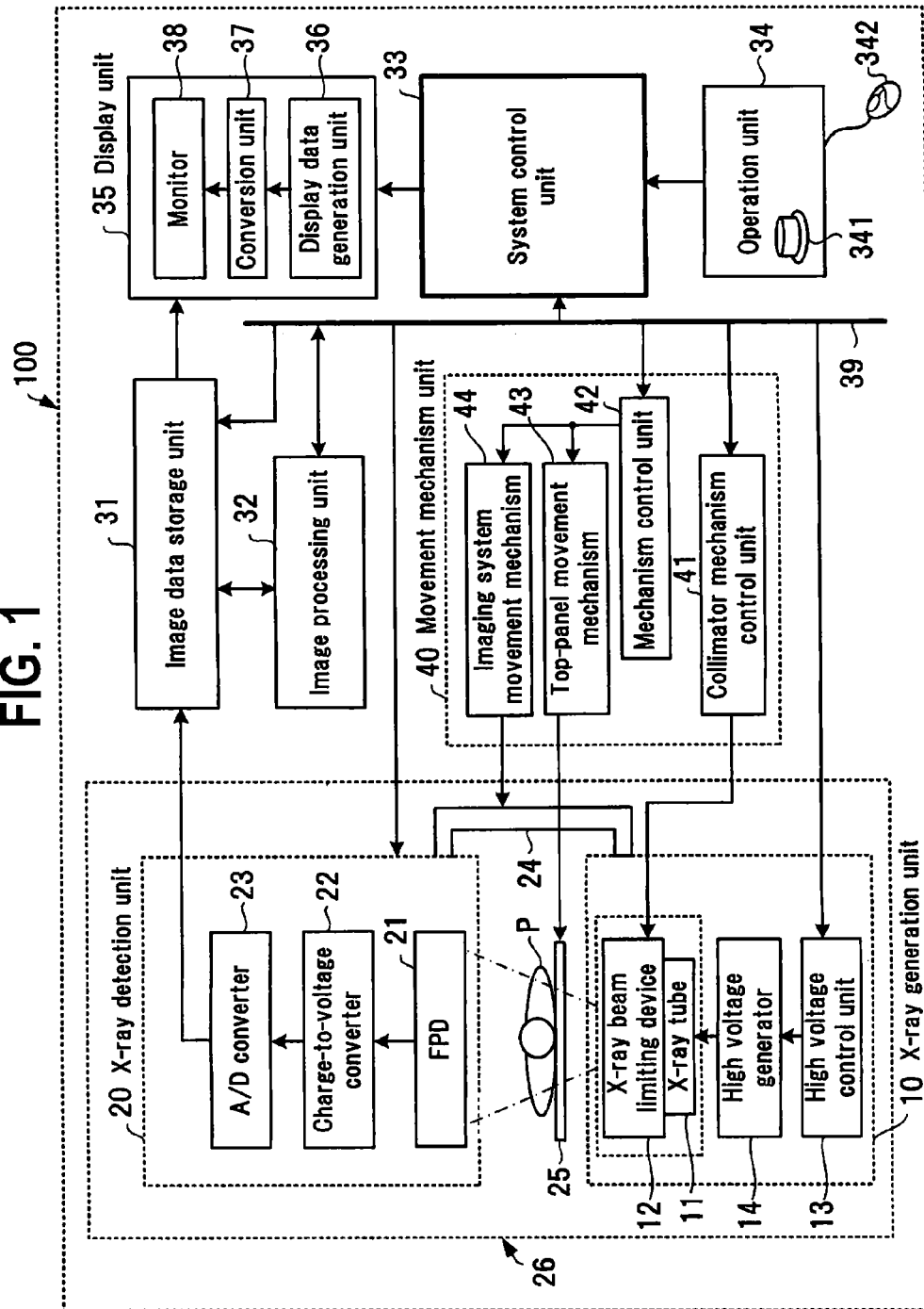


FIG. 2

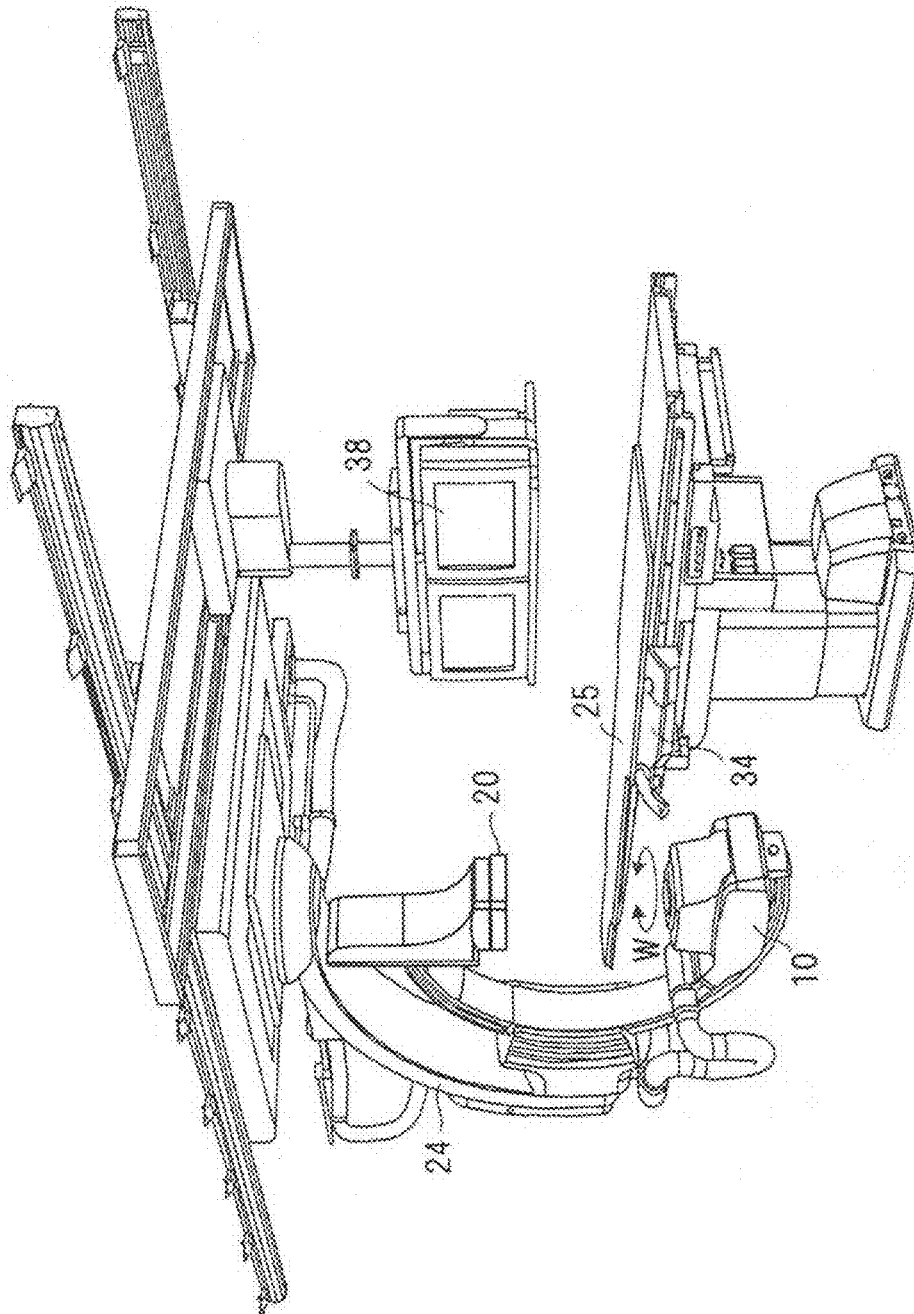


FIG.3A

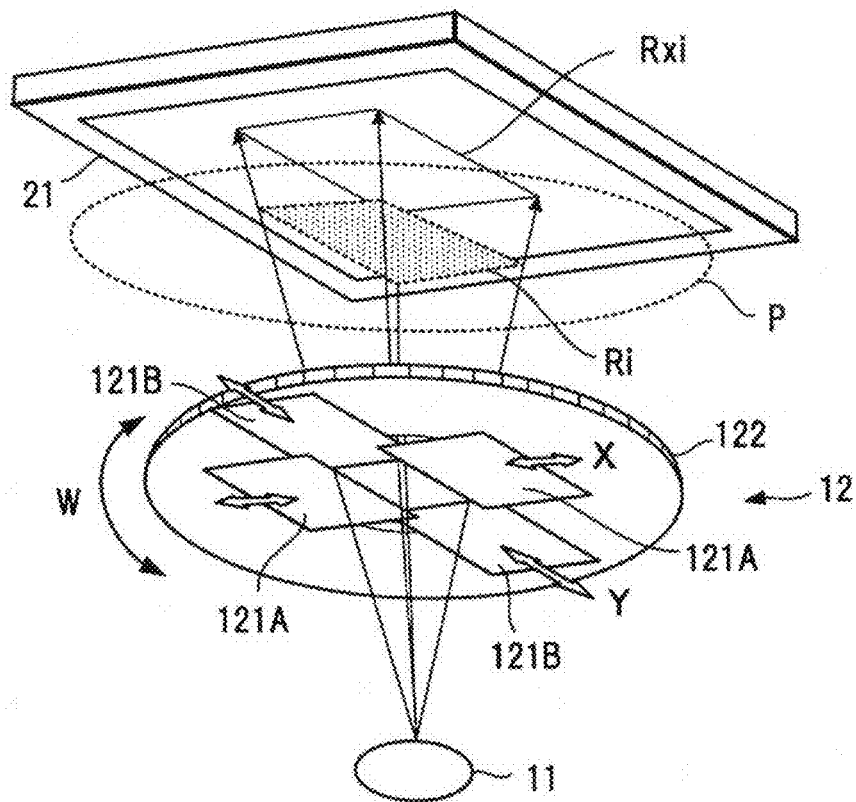


FIG.3B

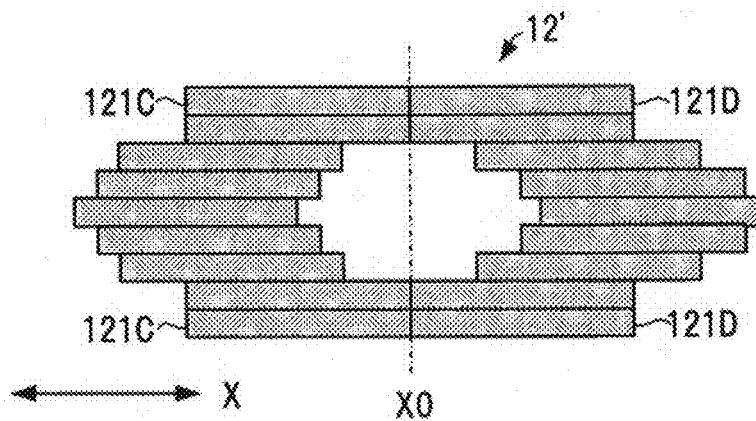


FIG.4

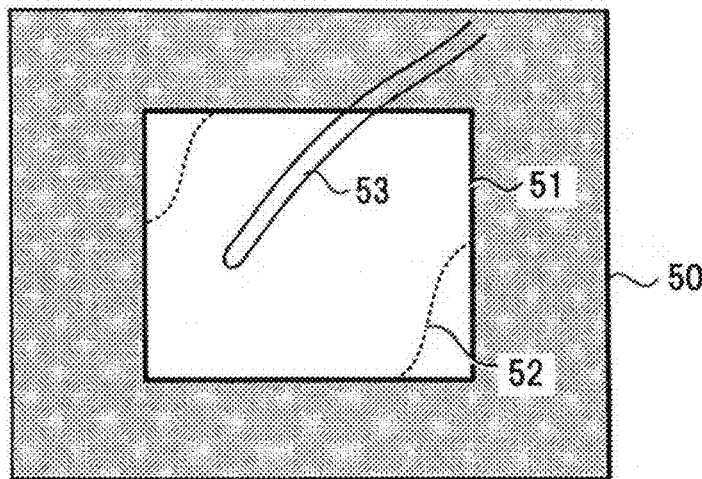


FIG. 5A

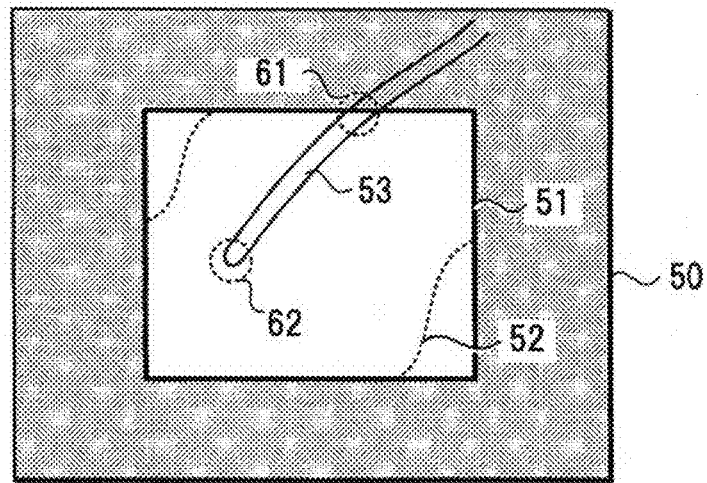


FIG. 5B

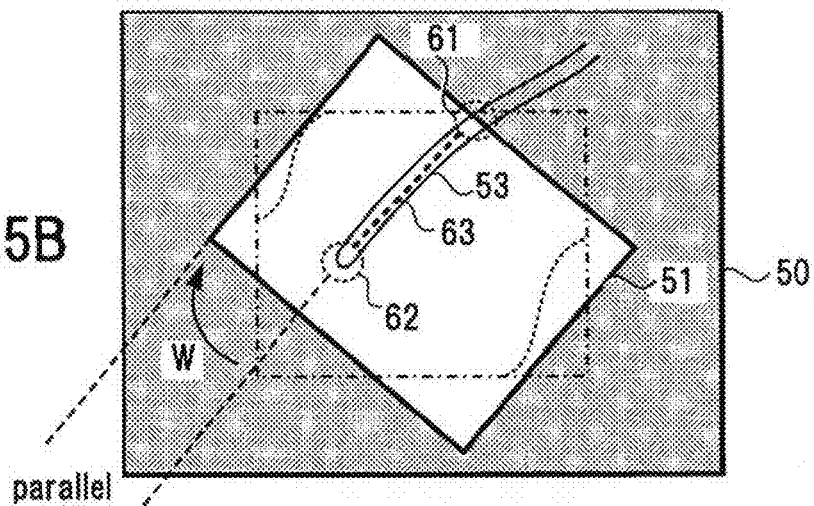


FIG. 5C

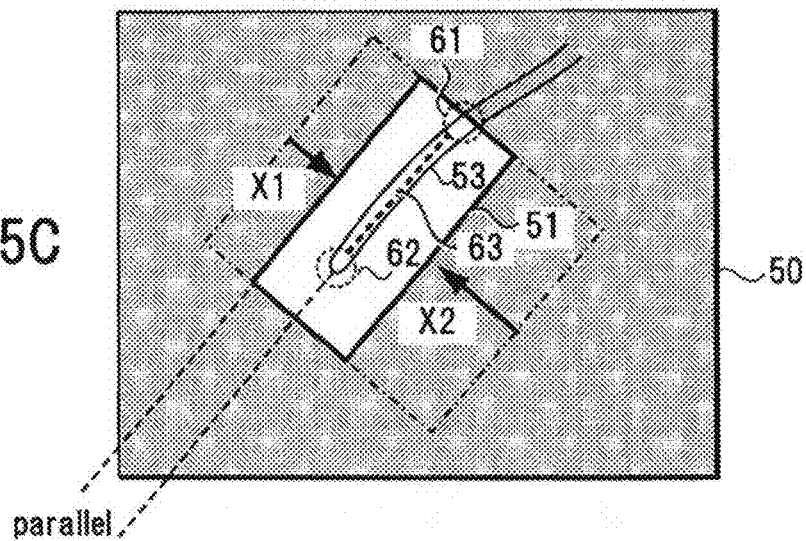


FIG.6A

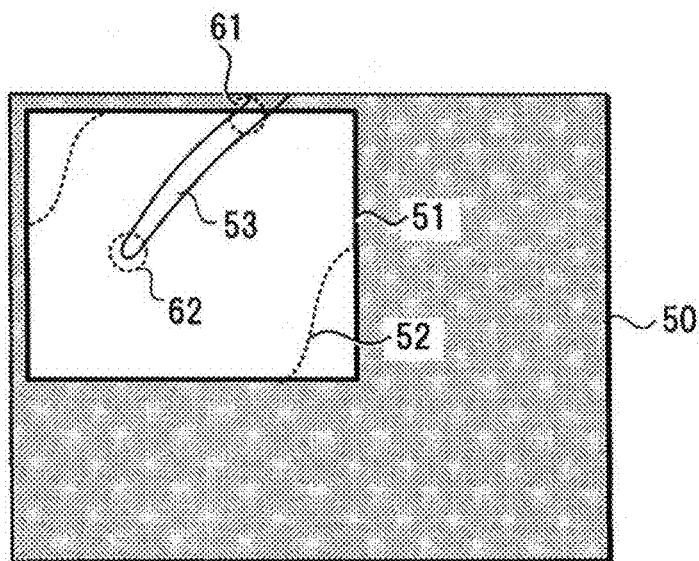


FIG.6B

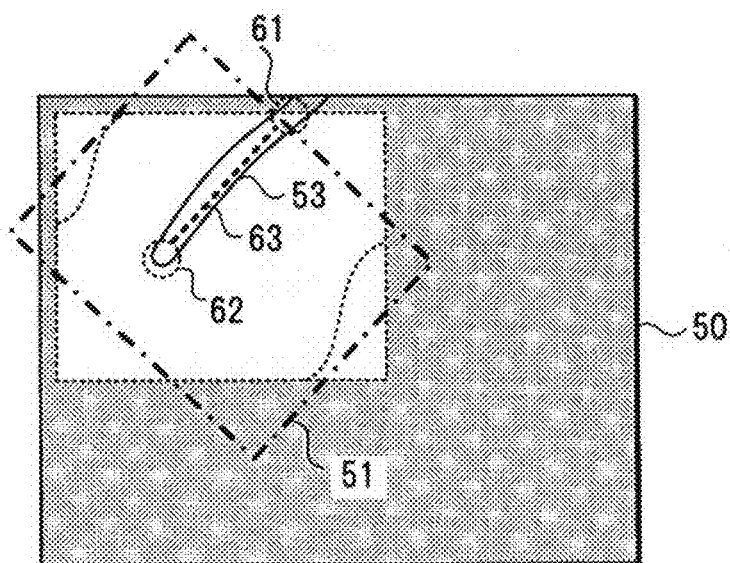


FIG. 7

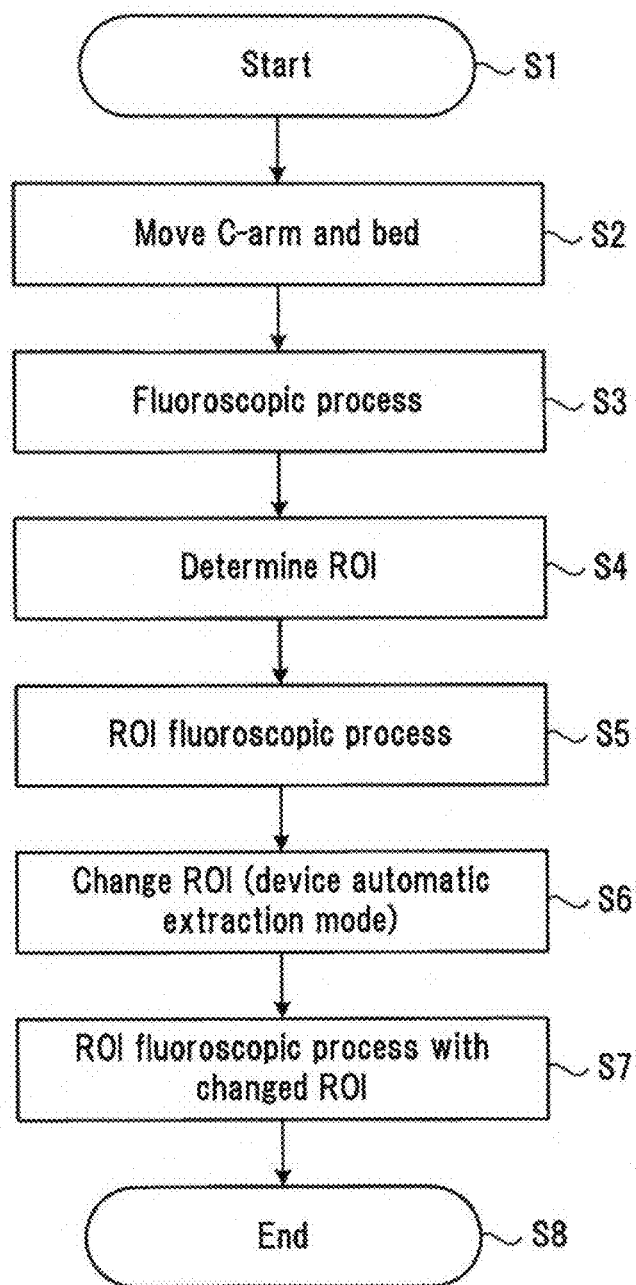


FIG. 8

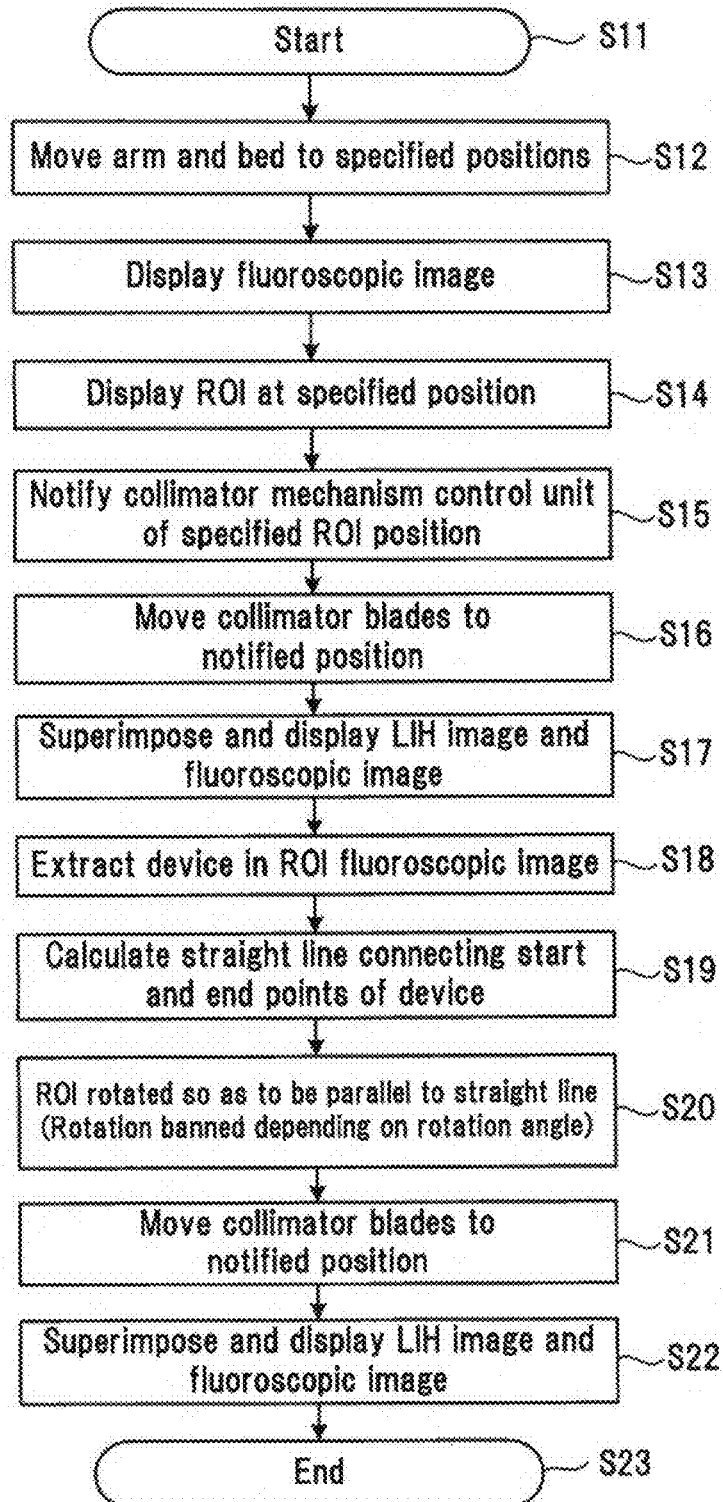


FIG. 9A

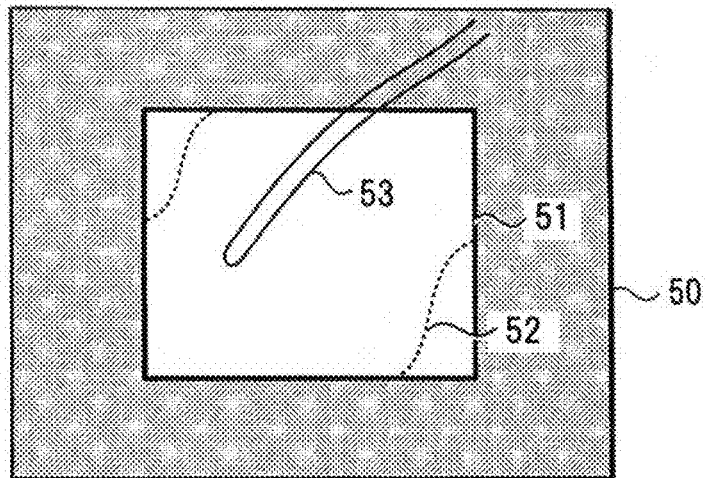


FIG. 9B

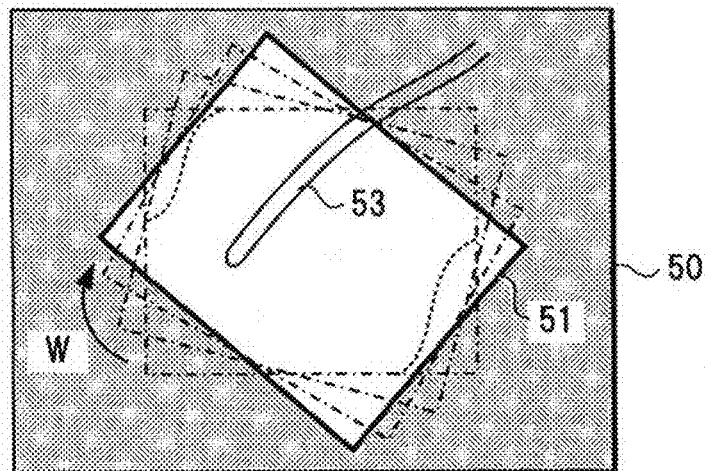


FIG. 9C

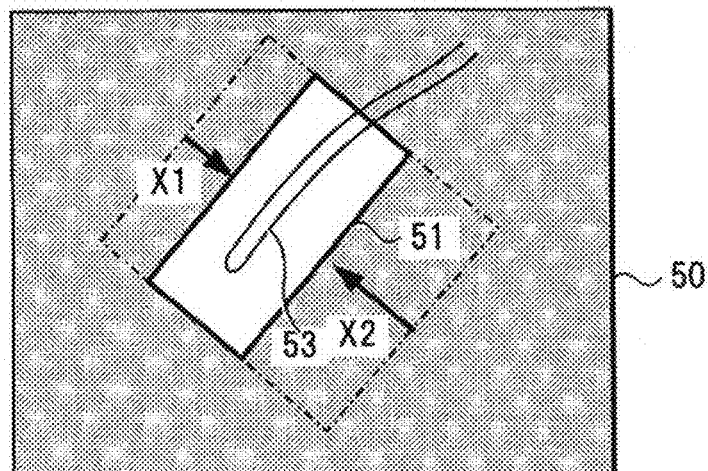


FIG.10

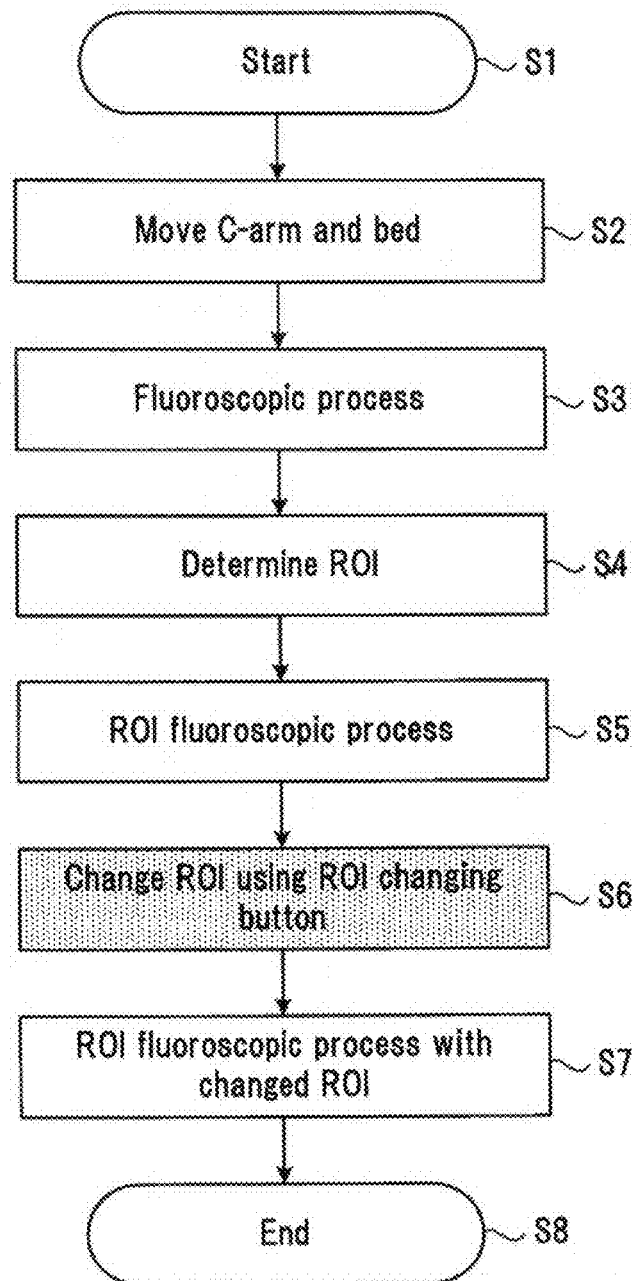


FIG. 11

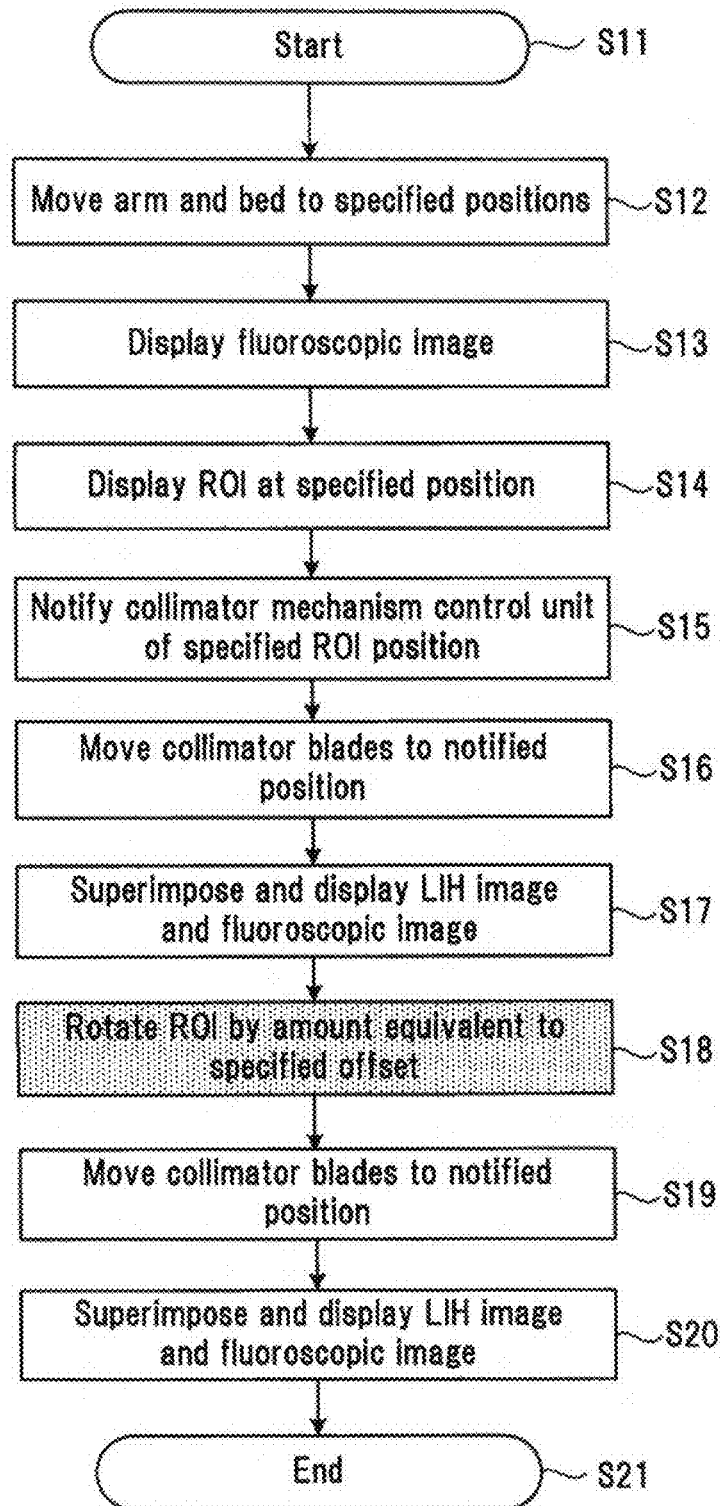


FIG.12A

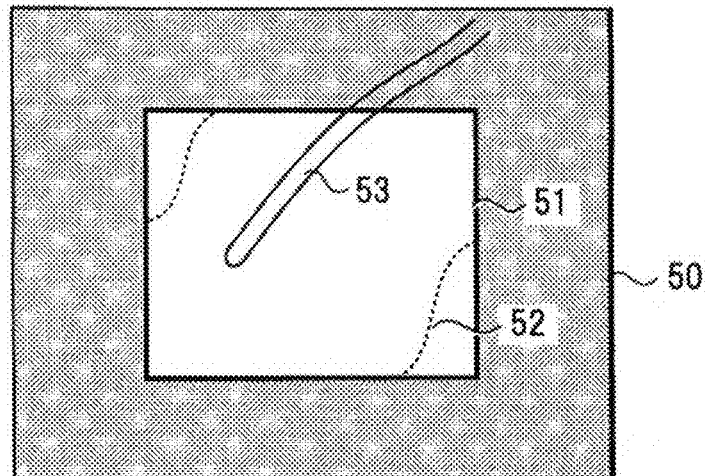


FIG.12B

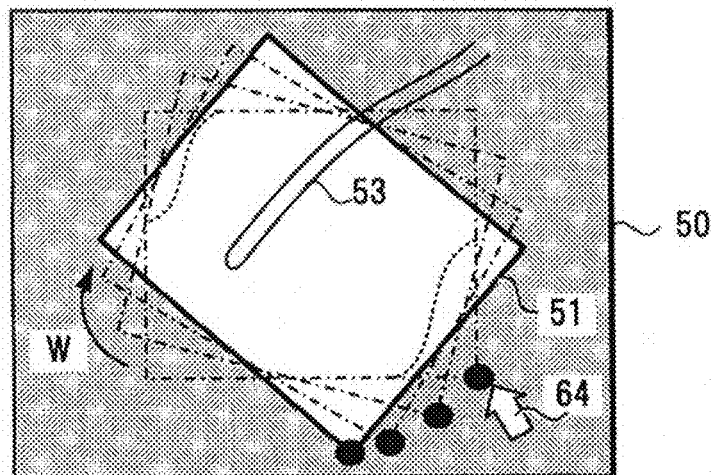


FIG.12C

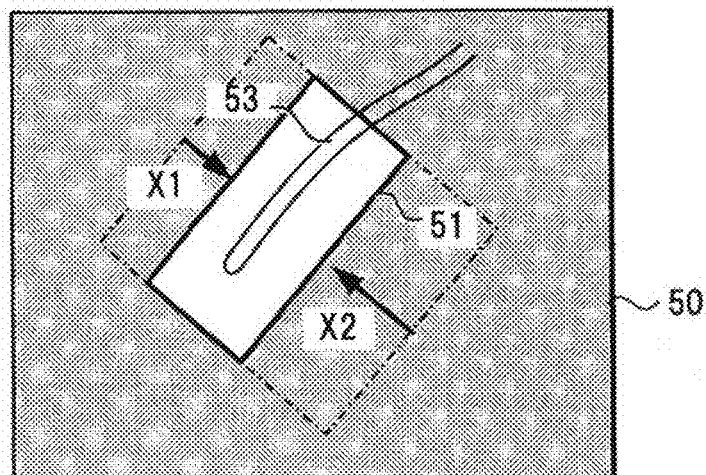


FIG.13A

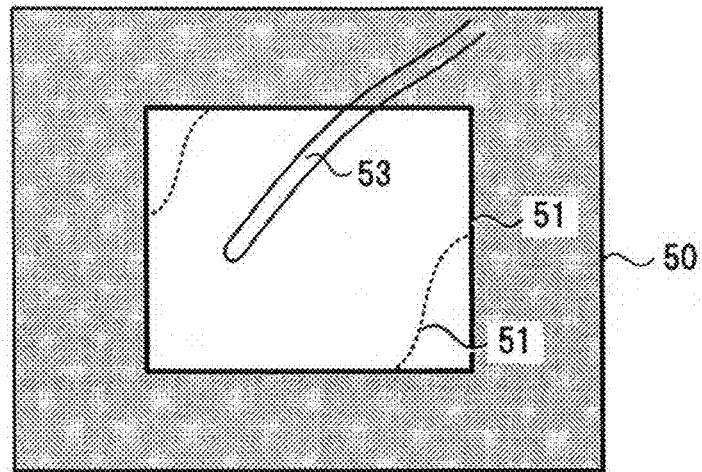


FIG.13B

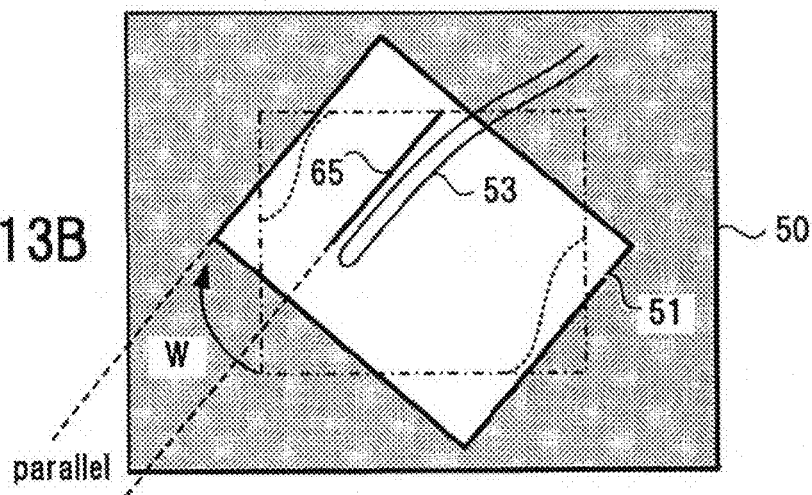


FIG.13C

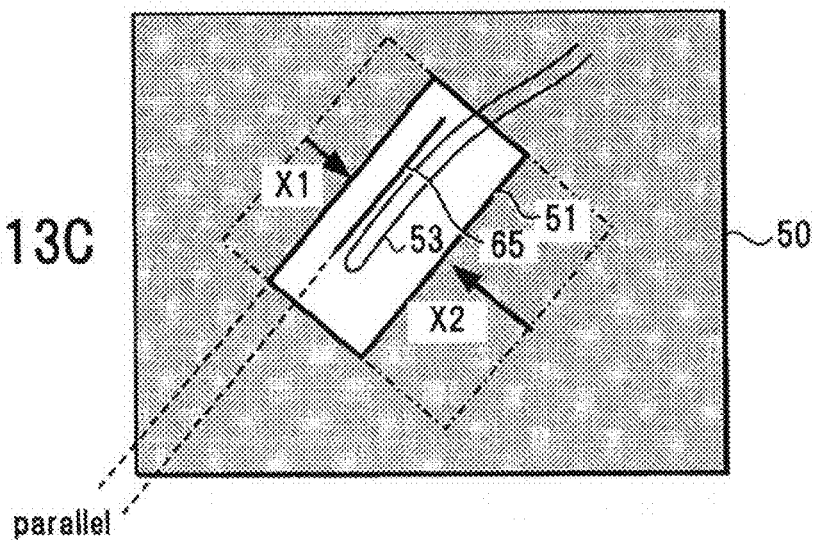


FIG. 14

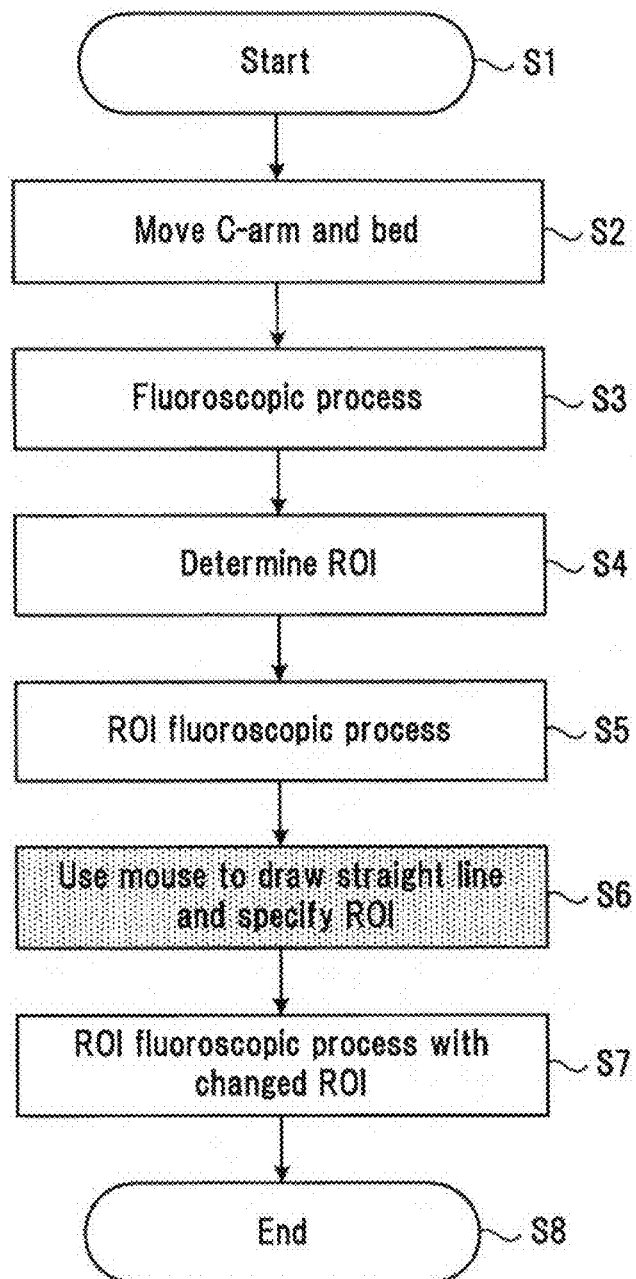
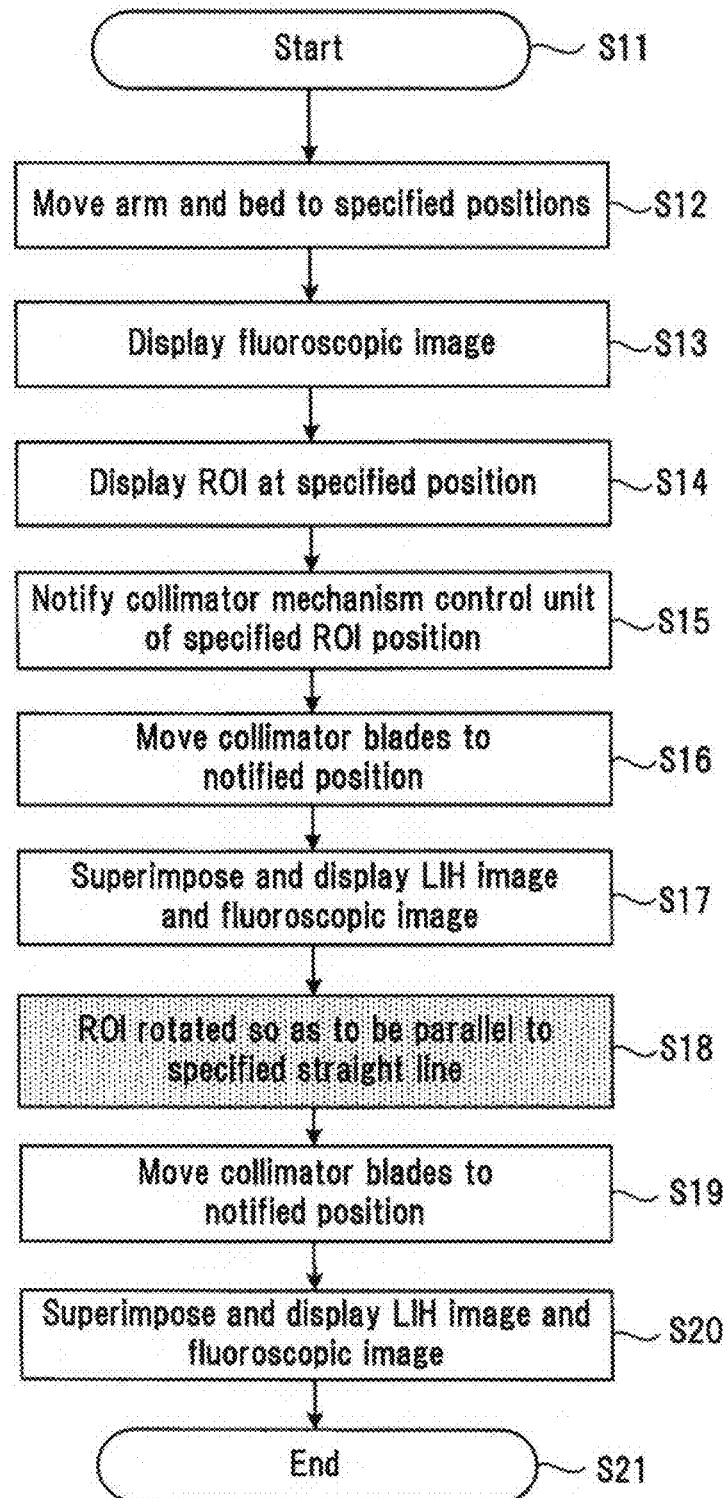


FIG. 15



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X-RAY DIAGNOSIS APPARATUS AND X-RAY DIAGNOSIS ASSISTING METHOD

CROSS-REFERENCE TO RELATED APPLICATION

This application is a continuation of International Application No. PCT/JP2013/002814, filed on Apr. 25, 2013, which is based upon and claims the benefit of priority from the prior Japanese Patent application No. 2012-119830, filed on May 25, 2012, the entire contents of which are incorporated herein by reference.

FIELD

Embodiments described herein relate to an X-ray diagnosis apparatus having an X-ray generation unit and an X-ray detector; and to an X-ray diagnosis apparatus that is designed to reduce an exposure dose by rotating and moving collimator blades of an X-ray beam limiting device in a way that narrows an irradiation field, and an X-ray diagnosis assisting method.

BACKGROUND

Conventionally, in endovascular treatment, angiographic examination, and the like, a catheter is inserted into a blood vessel, for example, from the base of a foot, and is brought to a target site via the blood vessel. When the catheter (or a guide wire that guides the catheter) is brought to the target site, an X-ray fluoroscopic image is displayed. Watching the displayed image, a user moves the catheter or the guide wire to an affected site.

In an X-ray diagnosis apparatus, an X-ray tube and an X-ray detector (which is generally a planar detector called FPD) are so disposed as to face each other, and, on a front of the X-ray tube, an X-ray beam limiting device is provided. The X-ray beam limiting device includes collimator blades that can slide. As the collimator blades are moved, a diagnosis area of a subject is selectively irradiated with X-rays. In this manner, the X-ray diagnosis apparatus is designed to protect the subject from unnecessary X-ray exposure.

However, the X-ray beam limiting device can move only in a horizontal direction (X-direction) and a vertical direction (Y-direction) with respect to FPD. If a blood vessel region that a user wants to see extends diagonally with respect to FPD (e.g., a blood vessel at the base of a foot), the problem arises that the irradiation field becomes larger, causing unnecessary exposure.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram showing the configuration of an X-ray diagnosis apparatus according to one embodiment;

FIG. 2 is a perspective view showing the overall configuration of an X-ray diagnosis apparatus according to one embodiment;

FIGS. 3A and 3B are schematic configuration diagrams of an X-ray beam limiting device according to one embodiment;

FIG. 4 is an explanatory diagram showing one example of an X-ray fluoroscopic image according to one embodiment;

FIGS. 5A to 5C are explanatory diagrams showing a ROI changing process according to one embodiment;

FIGS. 6A and 6B are explanatory diagrams showing other examples of displaying an X-ray fluoroscopic image according to one embodiment;

FIG. 7 is a workflow diagram showing a ROI changing process of one embodiment from user's point of view;

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FIG. 8 is a workflow diagram showing a ROI changing process of one embodiment from system's point of view;

FIGS. 9A to 9C are explanatory diagrams showing a ROI changing process according to a second embodiment;

FIG. 10 is a workflow diagram showing a ROI changing process of the second embodiment from user's point of view;

FIG. 11 is a workflow diagram showing a ROI changing process of the second embodiment from system's point of view;

FIGS. 12A to 12C are explanatory diagrams showing a ROI changing process according to a modified example of the second embodiment;

FIGS. 13A to 13C are explanatory diagrams showing a ROI changing process according to a third embodiment;

FIG. 14 is a workflow diagram showing a ROI changing process of the third embodiment from user's point of view; and

FIG. 15 is a workflow diagram showing a ROI changing process of the third embodiment from system's point of view.

DETAILED DESCRIPTION

An X-ray diagnosis apparatus of an embodiment includes: an imaging unit that includes an X-ray tube which emits an X-ray to a subject, and an X-ray detector which detects an X-ray passing through the subject; an X-ray beam limiting unit that is disposed between the X-ray tube and the X-ray detector has a plurality of collimator blades, and can be rotated; an image processing unit that generates a fluoroscopic image of a region of interest set by the X-ray beam limiting unit; and a control unit that individually controls the plurality of collimator blades in such a way that a long side of an opening formed by the plurality of collimator blades goes in a longitudinal direction of a target within the fluoroscopic image.

Hereinafter, an X-ray diagnosis apparatus of one embodiment will be described in detail with reference to the accompanying drawings. Incidentally, the same portions in each diagram are represented by the same reference symbols.

First Embodiment

FIG. 1 is a block diagram showing the configuration of an X-ray diagnosis apparatus according to one embodiment. FIG. 1 shows an X-ray diagnosis apparatus 100 called an angiography apparatus. The X-ray diagnosis apparatus 100 includes an X-ray generation unit 10, which generates an X-ray for a subject P, and an X-ray detection unit 20. The X-ray detection unit 20 detects an X-ray that has passed through the subject P in a two-dimensional manner, and generates X-ray projection data on the basis of the detection result.

The X-ray generation unit 10 includes an X-ray irradiation unit, which has an X-ray tube 11 and an X-ray beam limiting device 12 (X-ray beam limiting unit), and a high voltage control unit 13, and a high voltage generator 14. The X-ray tube 11 is a vacuum tube that generates an X-ray. The X-ray tube 11 is designed to accelerate electrons, which are emitted from a cathode (filament), using a high voltage to get the electrons colliding with a tungsten anode, thereby generating an X-ray. The high voltage control unit 13 controls the high voltage generator 14 in accordance with a command signal from a system control unit 33 (described later). That is, the system control unit 33 controls X-ray irradiation conditions, including a tube current and tube voltage of the X-ray tube 11, an X-ray pulse width, an irradiation period, an imaging section, and an irradiation time.

The X-ray detection unit **20** includes a FPD **21** (Flat Panel Detector); a charge-to-voltage converter **22** which converts electric charge read from the FPD **21** to voltage; and an A/D converter **23** which converts an output of the charge-to-voltage converter **22** to a digital signal. From the A/D converter **23**, X-ray projection data is output. The FPD **21** constitutes an X-ray detector. The X-ray generation unit **10** and the X-ray detection unit **20** are supported by an arm (C-arm) **24**. The C-arm **24** is able to move in a body-axis direction of the subject P placed on a top panel **25** of a bed. The C-arm **24** is also able to rotate around the body axis of the subject P. Incidentally, the X-ray generation unit **10** and the X-ray detection unit **20** constitute an imaging unit **26**. As the C-arm **24** is rotated, the imaging unit **26** rotates around the subject P, imaging of the subject P from different angular directions.

The X-ray diagnosis apparatus **100** includes an image data storage unit **31**, an image processing unit **32**, the system control unit **33**, an operation unit **34**, and a display unit **35**. In the image data storage unit **31**, X-ray projection data from the A/D converter **23** is sequentially stored, and image data is generated. The image processing unit **32** performs imaging processing and calculation on the generated image data when needed in order to achieve objectives such as edge enhancement and improved S/N. Results of the image processing and calculation are stored in the image data storage unit **31**. The image data stored in the image data storage unit **31** is read when necessary, and is supplied to the display unit **35** where the image data is displayed.

The system control unit **33** includes a CPU and a storage circuit (not shown), and runs on the basis of input information, setting information, and selection information from the operation unit **34**. The system control unit **33** constitutes a control unit that takes overall control of each unit of the X-ray diagnosis apparatus **100** via a bus line **39**.

The operation unit **34** allows users, such as a doctor or examiner, to input various commands and perform other operations. The operation unit **34** includes input devices, such as an operation button **341**, a mouse **342**, a switch, a keyboard, a trackball, and a joystick; an interactive interface equipped with a display panel, various switches, or the like. The operation unit **34** enables setting of a movement direction and movement speed of the top panel **25**; a rotation/movement direction and rotation/movement speed of the imaging unit; and X-ray irradiation conditions, including the tube voltage and the tube current.

In order to display image data, the display unit **35** includes a display data generation unit **36**, a conversion unit **37**, and a monitor **38**. The display data generation unit **36** combines image data with supplementary information, or converts image data into a predetermined display format to generate display data. The conversion unit **37** performs D/A (Digital/Analog) conversion and television format conversion on the display data to generate video signals. The generated video signals are displayed on the monitor **38**, which is a liquid crystal monitor or the like.

The X-ray diagnosis apparatus **100** also includes a movement mechanism unit **40**. The movement mechanism unit **40** includes a collimator mechanism control unit **41** and a mechanism control unit **42**. The collimator mechanism control unit **41** controls the movement of collimator blades and other parts of the X-ray beam limiting device **12**, and controls rotation of the X-ray beam limiting device **12**. The mechanism control unit **42** controls a movement mechanism **43** of the top panel **25** on which the subject P is placed. The mechanism control unit **42** also controls an imaging system movement mechanism **44** of the imaging unit **26**, C-arm **24**, and the like. The movement mechanism unit **40** operates in response

to an operation of the operation unit **34**, and controls movements of each part under the control of the system control unit **33**.

FIG. 2 is a perspective view showing the overall configuration of the X-ray diagnosis apparatus **100** (angiography apparatus). In FIG. 2, the X-ray generation unit **10** and the X-ray detection unit **20** are supported by the C-arm **24** so as to face each other. A bed is disposed for the C-arm **24**. On the top panel **25** of the bed, a subject (not shown) is placed. The position and height of the top panel **25** is controlled by the mechanism control unit **42**. While the X-ray generation unit **10** faces the X-ray detection unit **20**, the X-ray beam limiting device **12** is able to rotate as indicated by arrow W. The X-ray beam limiting device **12** can rotate independently of the FPD **21**.

The C-arm **24** is supported by a rail provided on a ceiling section, for example. The C-arm **24** can move in a body-axis direction, from the head of the subject to the leg. As the C-arm **24** is rotated, the imaging unit **26** (the X-ray generation unit **10** and the X-ray detection unit **20**) rotates around the body axis of the subject. The imaging unit **26** can slide and rotate along the C-arm **24**.

X-ray projection data is processed by the image processing unit **32**, and image data is displayed on the monitor **38**. The monitor **38** is attached to the ceiling section, for example. To the bed, the operation unit **34** is attached. In response to an operation of the operation unit **34**, the system control unit **33** controls the height of the top panel **25**, and the movement and rotation of the C-arm **24**; adjusts an irradiation range of an X-ray; controls an irradiation timing; and performs other operations.

FIG. 3A is a schematic configuration diagram (perspective view) of the X-ray beam limiting device **12**. As shown in FIG. 3A, the X-ray beam limiting device **12** is designed to regulate an X-ray irradiation region of the subject P. The X-ray beam limiting device **12** includes collimator blades **121A** and **121B** that enable a partial imaging region, which is set within an imageable region of the FPD **21**, to be irradiated with a cone beam emitted from the X-ray tube **11**. The collimator blades **121A** and **121B** can move in directions indicated by arrows X and Y as shown in FIG. 3A. The collimator blades **121A** and **121B** are moved by the collimator mechanism control unit **41**. In this manner, the position and size of an opening is arbitrarily changed, and a region of interest is set.

As a result, an opening is formed by the collimator blades **121A** and **121B**. An imaging region RXi of the FPD **21** is formed by an X-ray that has passed through the opening and the region of interest Ri of the subject P. The FPD **21** converts the X-ray that has passed through the region of interest Ri of the subject P into electric charges, and accumulates the electric charges. By reading the accumulated electric charges, the FPD **21** generates X-ray projection data.

The collimator blades **121A** and **121B** are supported by a rotation unit **122**. The collimator mechanism control unit **41** rotates the rotation unit **122** around an optical axis of the X-ray, thereby rotating an opening formed by the collimator blades **121A** and **121B**. In this manner, the angle of the imaging region RXi of the FPD **21** can be changed.

The X-ray beam limiting device **12** (X-ray beam limiting unit) is not limited to that in the example shown in FIG. 3A. For example, an X-ray beam limiting device **12'** of a multi-leaf type may be used as shown in FIG. 3B. FIG. 3B is a schematic configuration diagram (plane view) of the X-ray beam limiting device **12'** of a multi-leaf type. The X-ray beam limiting device **12'** includes a plurality of leaves **121C** and **121D**, which can freely advance and retreat along an X-axis and are in a rectangular shape.

A plurality of leaves **121C** and **121D** constitute collimator blades. Two leaves **121C** and **121D** on both sides of a central axis **X0** are paired. The two leaves **121C** and **121D** that are paired are moved along the X-axis to turn the opening (irradiation field) into any shape other than a rectangular shape. When the multi leaf-type X-ray beam limiting device **12'** is supported on the rotation unit **122**, the X-ray beam limiting device **12'** can be rotated in the direction of 'W'. The X-ray beam limiting device **12** shown in FIG. 3A, and the multi leaf-type X-ray beam limiting device **12'** shown in FIG. 3B may be used in combination.

The following describes how to control an X-ray beam limiting device of the embodiment, as well as an example of displaying a fluoroscopic image. Incidentally, what is described below is the case where the X-ray beam limiting device **12** shown in FIG. 3A is used.

For example, in endovascular treatment, angiographic examination, and the like, a device, such as a catheter or a guide wire that guides the catheter, is inserted into a blood vessel, and is brought to a target site via the blood vessel. When the device is brought to the target site, an X-ray fluoroscopic image is displayed. Watching the displayed image, a user moves the device to an affected site.

According to the embodiment, first, the subject **P** is placed on the top panel **25**, and the C-arm **24** and the top panel **25** are moved to a specified position. The subject **P** is then irradiated with an X-ray, and a fluoroscopic image is displayed. The term "fluoroscopic" means a process of emitting an X-ray with a small radiation dose and providing moving pictures in real time, assisting a user in positioning of a patient or endovascular treatment. Watching the fluoroscopic image, a user determines a region of interest (ROI) to see therethrough. That is, the LIH (Last Image Hold) image that the user sees through is used as a background image. The fluoroscopic image (ROI fluoroscopic image), which is obtained as the irradiation field is narrowed by the collimator blades **121A** and **121B** of the X-ray beam limiting device **12**, is superimposed on the LIH image to be displayed.

FIG. 4 shows one example of an X-ray fluoroscopic image displayed on the monitor **38**. In FIG. 4, on a display screen **50** of the monitor **38**, an ROI fluoroscopic image **51** is displayed. On the ROI fluoroscopic image **51**, a LIH image **52** is displayed as a background image. Because of the fluoroscopic image, a device image **53** is displayed.

The ROI is specified as a user (doctor or examiner) operates the operation section **34**. Information about the specified ROI is transmitted to the collimator mechanism control unit **41** via the system control unit **33**. The collimator mechanism control unit **41** controls the positions of the collimator blades **121A** and **121B** of the X-ray beam limiting device **12** to narrow the irradiation field. The above has described general settings of the ROI.

FIGS. 5A to 5C are diagrams illustrating a ROI changing process. As shown in FIG. 5A, on the fluoroscopic image (ROI fluoroscopic image) **51** which is obtained as the irradiation field is narrowed by the collimator blades **121A** and **121B**, the image **53** of a device which is a target, is displayed. The ROI is set around the position of the device.

If the device such as catheter, extends diagonally (due to a blood vessel at the base of a foot or the like, for example), the collimator blades **121A** and **121B** can move only in the X- and Y-directions even as the irradiation field is narrowed by the collimator blades **121A** and **121B**. Accordingly, in order to confirm the entire device that extends diagonally on the fluoroscopic image, the region of interest needs to become larger, causing unnecessary exposure for the subject **P**.

Therefore, according to the first embodiment, as shown in FIG. 5A, what is calculated is a straight line **63** connecting a start point **61** and endpoint **62** of the device image **53** in the ROI fluoroscopic image **51**. The image processing unit **32** calculates the straight line **63**. That is, the image processing unit **32** detects, based on image data of the ROI fluoroscopic image **51**, the device image **53** to obtain coordinates of the start point **61** and endpoint **62** of the device image **53** in the ROI fluoroscopic image **51**. Then, as shown in FIG. 5B, the image processing unit **32** calculates components of the line (straight line **63**) connecting the start point **61** and the end point **62**. The straight line **63** is a line that runs parallel to the longitudinal direction of the target (device image **53**).

Then, the image processing unit **32** rotates the ROI (or a frame of the ROI image **51**), so that one side of the ROI runs parallel to the calculated straight line **63**. That is, one side of the ROI becomes parallel to the longitudinal direction of the device image **53**. Information about the rotated ROI is transmitted to the collimator mechanism control unit **41**. Incidentally, if one side of the ROI is parallel to the calculated straight line **63** in the first place, there is no need to rotate the ROI.

As shown in FIG. 5C, the collimator mechanism control unit **41** rotates the rotation unit **122** (FIG. 3A) of the X-ray beam limiting device **12** around the optical axis in the direction of 'W'. Moreover, in a direction perpendicular to the straight line **63** (device image **53**), the positions of the collimator blades **121A** and **121B** are controlled in such a way as to move closer to the straight line **63**. For example, the positions of the collimator blades **121A** are moved in X1- and X2-directions to change the ROI.

As a result, the ROI becomes smaller, and the ROI fluoroscopic image **51**, too becomes smaller in size, thereby reducing radiation exposure for the subject **P**. Even as the ROI becomes smaller, the device image **53** is displayed without any problem, assisting the progression of the device.

The collimator blades **121A** and **121B** are set in advance so as to approach a preset distance from the straight line **63**. Therefore, the ROI can be automatically changed. Accordingly, even when the device image **53** extends diagonally, the X-ray beam limiting device **12** is rotated in accordance with the inclination angle of the device image **53**, and the positions of the collimator blades **121A** and **121B** are controlled. In this manner, the ROI can be changed.

Incidentally, FIG. 5C shows an example in which the changed ROI is in a rectangular shape. However, if the multi leaf-type X-ray beam limiting device **12'** shown in FIG. 3B is used, the ROI may be changed not only into a rectangular shape, but also into an elongated elliptical shape.

FIGS. 6A and 6B are diagrams showing the ROI fluoroscopic image **51** of the case where the ROI is away from the center of the FPD **21**. As shown in FIG. 6A, when the ROI is away from the center of the FPD **21**, the straight line **63** connecting the start point **61** and end point **62** of the device image **53** in the ROI fluoroscopic image **51** appears at a corner of the FPD **21**. If the ROI is rotated, as shown in FIG. 6B, an X-ray is emitted to outside the FPD **21**. Therefore, if a region outside the FPD **21** is irradiated with an X-ray as the ROI is rotated, the rotation is stopped.

FIG. 7 is a workflow diagram showing a ROI changing process from user's point of view. In FIG. 7, step **S1** is a start step. At step **S2**, the subject **P** is placed on the top panel **25** of the bed, and the C-arm **24** and the top panel **25** are moved. At step **S3**, an X-ray is emitted to the subject **P** to carryout a fluoroscopic process. At the next step **S4**, the user determines the ROI while watching the fluoroscopic image.

At step **S5**, which follows a process of determining the ROI, a ROI fluoroscopic process is carried out. At step **S6**, the

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procedure described in FIGS. 5A to 5C is used to automatically extract the device image 53 and change the ROI. At step S7, the changed ROI is used to carry out a ROI fluoroscopic process. Checking the position of the device, the user moves the device forward. Step S8 is an end step.

FIG. 8 is a workflow diagram showing a ROI changing process from system's point of view. In FIG. 8, step S11 is a start step. At step S12, the C-arm 24 and the top panel 25 are moved to specified locations. At step S13, an X-ray is emitted to the subject P to carry out a fluoroscopic process, and a fluoroscopic image is displayed on the monitor 38. At step S14, at a specified position of the display screen 50 of the monitor 38, the ROI is displayed. At step S15, the collimator mechanism control unit 41 is notified of the position of the specified ROI.

At step S16, the collimator mechanism control unit 41 moves the collimator blades 121A and 121B to the notified position. At step S17, the LIH image 52 and the ROI fluoroscopic image 51 are superimposed and displayed on the display screen 50 (see FIG. 5A). At the next step S18, the device image 53 in the ROI fluoroscopic image 51 is detected and extracted. At step S19, the straight line 63 connecting the start point 61 and end point 62 of the device image is calculated. At step S20, the ROI is so rotated that one side of the ROI becomes parallel to the straight line 63 (see FIG. 5B). However, if the rotation angle is such that an X-ray is emitted to outside the FPD 21 as described in FIG. 6, the rotation is banned. For example, a warning, such as the message "rotation is impossible," may be issued.

At step S21, as the ROI is rotated, the collimator mechanism control unit 41 is notified of new ROI information. The collimator mechanism control unit 41 moves the collimator blades 121A and 121B to the notified position. At step S22, the ROI fluoroscopic image 51, which is designed to see through with the changed ROI is superimposed on the LIH image 52, and is displayed (see FIG. 5C). Step S23 is an end step.

According to the above-described first embodiment, the device image within the ROI is automatically detected, and the ROI is so rotated as to be substantially parallel to the device image. Then, the ROI is so changed as to exist in a preset region around the device. Therefore, it is possible to reduce radiation exposure for the subject P.

Second Embodiment

The following describes an X-ray diagnosis apparatus according to a second embodiment. According to the second embodiment, a user operates a button to order rotation of the X-ray beam limiting device 12. FIGS. 9A and 9C are diagrams illustrating a ROI changing process according to the second embodiment.

As shown in FIG. 9A, on the ROI fluoroscopic image 51, which is obtained as the irradiation field is narrowed by the collimator blades 121A and 121B, the image 53 of a device which is a target, is displayed. As shown in FIG. 9B, a user operates the operation unit 34 to rotate the ROI (or a frame of the ROI image 51). The image processing unit 32 transmits information about the rotated ROI to the collimator mechanism control unit 41 via the system control unit 33.

For example, in the operation unit 34, an operation button 341 is provided to enable a user to order the rotation of the ROI. Each time the user pushes the operation button 341, the ROI is rotated by an amount equivalent to a predetermined offset. The user rotates the ROI until one side of the ROI reaches an angle at which the side is substantially parallel to the device image 53. After the user pushes a decision key (not

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shown), the rotation is stopped. Incidentally, the operation button 341 which enables a user to order the rotation, may be a dial button, the ROI is rotated in accordance with the rotation direction and rotation angle of the dial button.

As shown in FIG. 9C, the collimator mechanism control unit 41 receives the information about the rotated ROI, and rotates the rotation unit 122 of the X-ray beam limiting device 12 in the direction of 'W'. In response to an operation by the user, the collimator mechanism control unit 41 controls the positions of the collimator blades 121A and 121B. The collimator mechanism control unit 41 brings the collimator blades 121A and 121B closer to the device image 53 in changing the ROI. For example, the collimator blades 121A are moved in the and X2-directions. As a result, the ROI fluoroscopic image 51 is changed in size, and the subject P's exposure to radiation is reduced.

Therefore, even when the device image 53 extends diagonally, the operation by the user makes it possible to rotate the X-ray beam limiting device 12 in accordance with the inclination angle of the device image 53, and control the positions of the collimator blades 121A and 121B to change the ROI.

Incidentally, as shown in FIG. 6A, if the ROI is away from the center of the FPD 21, and if an X-ray is emitted to outside the FPD 21 after the ROI is rotated, a warning message may be issued to urge a user to stop the rotation of the X-ray beam limiting device 12.

FIG. 10 is a workflow diagram showing a ROI changing process of the second embodiment from user's point of view. In the case of FIG. 10, steps S1 to S5 are the same as those of the first embodiment. However, step S6 is different.

That is, at step S6, the operation button 341 of the operation unit 34 is used to change the ROI. At step S7, the changed ROI is used to carry out a ROI fluoroscopic process. Moreover, at step S7, the user moves the device forward while checking the position of the device, and the process comes to an end at step S8.

FIG. 11 is a workflow diagram showing a ROI changing process of the second embodiment from system's point of view. In the case of FIG. 11, steps S11 to S17 are the same as those of the first embodiment. However, step S18 is different.

That is, at step S18, as the user operates the operation button 341, the ROI is rotated by an amount equivalent to a specified offset (see FIG. 9B). However, as described in FIG. 6B, if the rotation angle is such that an X-ray is emitted to outside the FPD 21, a message is issued to ban the rotation.

At the next step S19, as the ROI is rotated, the collimator mechanism control unit 41 is notified of new ROI information. The collimator mechanism control unit 41 moves the collimator blades 121A and 121B to the notified position (see FIG. 9C). At step S20, the ROI fluoroscopic image 51, which is designed to see through with the changed ROI, is superimposed on the LIH image 52, and is displayed. Step S21 is an end step.

FIGS. 12A to 12C are diagrams illustrating a ROI changing process of an X-ray diagnosis apparatus according to a modified example of the second embodiment. In the case of FIG. 12, a user operates a mouse 342 provided in the operation unit 34 to order rotation of the X-ray beam limiting device 12.

As shown in FIG. 12A, on the ROI fluoroscopic image 51, which is obtained as the irradiation field is narrowed by the collimator blades 121A and 121B, the device image 53 is displayed. As shown in FIG. 12B, a user operates the mouse 342 to rotate the ROI. The image processing unit 32 transmits information about the rotated ROI to the collimator mechanism control unit 41 via the system control unit 33.

Operating the mouse 342, the user positions a cursor 64 at a corner of the ROI fluoroscopic image 51 to move in a

rotation direction. By operating the mouse 342, the user can specify an angle by which the ROI is rotated, and a direction in which the ROI is rotated. The user rotates the ROI until one side of the ROI reaches a position where the side is substantially parallel to the device image 53.

Then, as shown in FIG. 12C, the collimator mechanism control unit 41 receives information about the rotated ROI, and rotates the rotation unit 122 of the X-ray beam limiting device 12 in the direction of 'W'. In response to an operation by the user, the collimator mechanism control unit 41 controls the positions of the collimator blades 121A and 121B. That is, the collimator blades 121A and 121B move in a direction that makes the collimator blades 121A and 121B closer to the device image 53, changing the ROI. As a result, the ROI fluoroscopic image 52 is decreased in size, and the subject P's exposure to radiation is reduced.

Incidentally, as shown in FIG. 6A, if the ROI is away from the center of the FPD 21, and if an X-ray is emitted to outside the FPD 21 after the ROI is rotated, a warning message may be issued to urge a user to stop the rotation of the X-ray beam limiting device 12.

In the example shown in FIGS. 12A to 12C, the same process as that shown in the workflow diagrams of FIG. 10 and FIG. 11 is performed. However, the process of step S6 of FIG. 10 is replaced with a process of "changing the ROI using the mouse." Moreover, the process of step S18 of FIG. 11 is replaced with a process of "rotating the ROI by an amount specified by the mouse."

As described above, according to the second embodiment, the user can rotate the ROI. The ROI can be so changed as to exist in a region around the device image. Therefore, it is possible to reduce radiation exposure for the subject P.

Third Embodiment

The following describes an X-ray diagnosis apparatus according to a third embodiment. According to the third embodiment, in response to an operation by a user, a parallel line is drawn near the device image 53. The drawn line is used to rotate the X-ray beam limiting device 12.

FIGS. 13A to 13C are diagrams illustrating a ROI changing process according to the third embodiment.

As shown in FIG. 13A, on the ROI fluoroscopic image 51, which is obtained as the irradiation field is narrowed by the collimator blades 121A and 121B, the device image 53 is displayed. Then, as shown in FIG. 13B, a user operates the mouse 342 to draw a straight line 65 near the device image 53 in such a way that the straight line 65 runs substantially parallel to a longitudinal direction of a mouse image 63. The image processing unit 32 determines which portion of the ROI fluoroscopic image 51 the straight line 65 is drawn in. When the straight line 65 is drawn, the ROI is rotated in such a way that one side of the ROI becomes parallel to the drawn straight line 65. The image processing unit 32 transmits information about the rotated ROI to the collimator mechanism control unit 41 via the system control unit 33.

As shown in FIG. 13C, the collimator mechanism control unit 41 rotates the rotation unit 122 of the X-ray beam limiting device 12 in the direction of 'W'. Moreover, in response to an operation by the user, the collimator mechanism control unit 41 controls the movements of the collimator blades 121A and 121B in such a way that the collimator blades 121A and 121B move closer to the device image 53, thereby changing the ROI. For example, the collimator blades 121A are moved in X1- and X2-directions. As a result, the ROI fluoroscopic image 51 is decreased in size, and the subject P's exposure to radiation is reduced.

Incidentally, the positions of the collimator blades 121A and 121B may be set in advance so as to approach a preset distance from the straight line 65. The ROI may be automatically changed with respect to the drawn straight line 65.

Therefore, even when the device image 53 extends diagonally, the X-ray beam limiting device 12 is rotated in accordance with the inclination angle of the device image 53, and the positions of the collimator blades 121A and 121B are controlled. In this manner, the ROI can be changed.

Incidentally, as shown in FIG. 6A, if the ROI is away from the center of the FPD 21, and if an X-ray is emitted to outside the FPD 21 after the ROI is rotated, a warning message may be issued to urge a user to stop the rotation of the X-ray beam limiting device 12.

FIG. 14 is a workflow diagram showing a ROI changing process of the third embodiment from user's point of view. In the case of FIG. 14, steps S1 to S5 are the same as those of the second embodiment. However, step S6 is different. That is, at step S6, as the mouse 342 of the operation unit 34 is operated, the straight line 65 is drawn near the device image 53, and the ROI is specified. At step 97, the changed ROI is used to carry out a ROI fluoroscopic process. Moreover, at step S7, the user moves the device forward while checking the position of the device, and the process comes to an end at step S8.

FIG. 15 is a workflow diagram showing a ROI changing process of the third embodiment from system's point of view. In the case of FIG. 15, steps S11 to S17 are the same as those of the second embodiment. However, step S18 is different.

That is, at step S18, the ROI is so rotated that the straight line 65 drawn by the user is parallel to one side of the ROI (see FIG. 13B). However, as described in FIG. 6, if the rotation angle is such that an X-ray is emitted to outside the FPD 21, a message is issued to ban the rotation.

At the next step S19, as the ROI is rotated, the collimator mechanism control unit 41 is notified of new ROI information. The collimator mechanism control unit 41 moves the collimator blades 121A and 121B to the notified position (see FIG. 13C). At step S20, the ROI fluoroscopic image 51, which is designed to see through with the changed ROI, is superimposed on the LIH image 52, and is displayed. The process comes to an end at step S21.

According to the above-described third embodiment, by drawing the line 65 that is substantially parallel to the device image within the ROI, the rotation angle of the ROI is specified. Moreover, the ROI is so changed as to exist in a preset region around the drawn line 65. Therefore, it is possible to reduce radiation exposure for the subject P.

In that manner, it is possible to assist the progression of the device, and reduce the subject's exposure to radiation.

While certain embodiments have been described, these embodiments have been presented by way of example only, and are not intended to limit the scope of the invention. Indeed, the novel apparatus and methods described herein may be embodied in a variety of other forms; furthermore, various omissions, substitutions and changes in the form of the apparatus and methods described herein may be made without departing from the spirit of the inventions. The accompanying claims and their equivalents are intended to cover such forms or modifications as would fall within the scope and spirit of the inventions.

What is claimed is:

1. An X-ray diagnosis apparatus comprising:
an imaging unit that includes an X-ray tube which emits an X-ray to a subject, and an X-ray detector which detects an X-ray passing through the subject;

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an X-ray beam limiting unit that is disposed between the X-ray tube and the X-ray detector, has a plurality of collimator blades, and can be rotated;

an image processing unit that detects a target based on an image data of a fluoroscopic image of a region of interest set by the X-ray beam limiting unit, and calculates components of a line of the target within the region of interest; and

a control unit that individually controls the plurality of collimator blades in such a way that a long side of an opening formed by the plurality of collimator blades goes in a longitudinal direction of the calculated components of the line within the fluoroscopic image.

2. The X-ray diagnosis apparatus according to claim 1, wherein:

the image processing unit generates a fluoroscopic image of a situation where a device is being inserted into the subject; and

the control unit regards an image of the device contained in the fluoroscopic image as the target, and controls rotation and movement of the plurality of collimator blades.

3. The X-ray diagnosis apparatus according to claim 2, wherein:

the image processing unit detects the device contained in a fluoroscopic image of the region of interest; and

the control unit controls rotation of the X-ray beam limiting unit in such a way that a long side of an opening formed by the plurality of collimator blades goes in a direction in which the device extends.

4. The X-ray diagnosis apparatus according to claim 2, wherein

the control unit rotates the X-ray beam limiting unit, and moves at least one of the collimator blades in such a way that the collimator blade approaches a preset distance from the target.

5. The X-ray diagnosis apparatus according to claim 1, wherein

the image processing unit uses a fluoroscopic LIH (Last Image Hold) image as a background image, and superimposes on the LIH image, a fluoroscopic image that is obtained as an irradiation field is narrowed by the X-ray beam limiting unit.

6. An X-ray diagnosis assisting method comprising:

including an imaging unit that includes an X-ray tube which emits an X-ray to a subject, and an X-ray detector which detects an X-ray passing through the subject;

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placing, between the X-ray tube and the X-ray detector, an X-ray beam limiting unit that has a plurality of collimator blades and can be rotated;

generating a fluoroscopic image of a region of interest set by the X-ray beam limiting unit;

detecting a target of the fluoroscopic image based on an image data of the region of interest;

calculating components of a line of the target within the region of interest; and

controlling individually the plurality of collimator blades in such a way that a long side of an opening formed by the plurality of collimator blades goes in a longitudinal direction of the components of the line within the fluoroscopic image.

7. The X-ray diagnosis assisting method according to claim 6, wherein:

generating a fluoroscopic image of a situation where a device is being inserted into the subject; and

controlling a rotation and movement of the plurality of collimator blades, an image of the device contained in the fluoroscopic image is regarded as the target.

8. The X-ray diagnosis assisting method according to claim 7, wherein:

detecting the device contained in a fluoroscopic image of the region of interest; and

rotating the X-ray beam limiting unit in such a way that a long side of an opening formed by the plurality of collimator blades goes in a direction in which the device extends.

9. The X-ray diagnosis apparatus according to claim 1, wherein

the image processing unit obtains coordinates of a start point and an end point of the target within the region of interest, and calculates a straight line connecting the start point and the end point as the components of the line.

10. The X-ray diagnosis assisting method according to claim 6, further comprising:

obtaining coordinates of a start point and an end point of the target within the region of interest; and

calculating a straight line connecting the start point and the end point as the components of the line.

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